

# Fast, low SAR and off-resonance insensitive T2 weighted Variable Amplitude PSIF (T2 VAPSIF) imaging

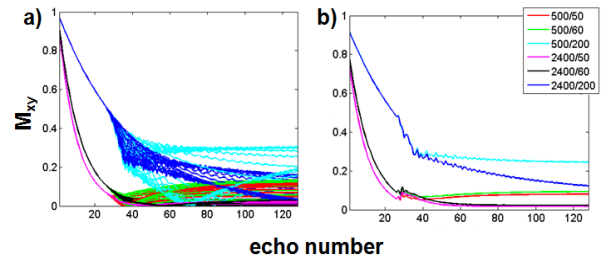
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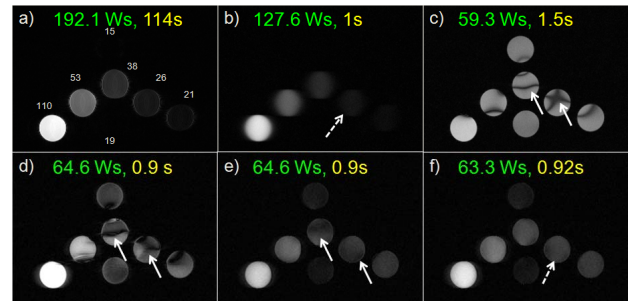
**Introduction:** T<sub>2</sub>-TIDE (Transition into Driven Equilibrium) [1] is a balanced SSFP (b-SSFP) sequence with a T<sub>2w</sub> transient acquisition. In this technique, the center of k-space is sampled using a spin-echo scheme (90°-180°-180°-...), to achieve T<sub>2w</sub>. While traversing towards the outer k-space lines, the flip angle is ramped down which reduces SAR, preserves signal and maintains edge resolution compared to Half Fourier Acquisition Single shot Turbo spin Echo (HASTE). However, T<sub>2</sub>-TIDE is sensitive to B<sub>0</sub> inhomogeneities, especially at high and ultra-high fields (>3T). In this work, we present a sequence called T<sub>2w</sub> Variable Amplitude PSIF (T<sub>2</sub>VAPSIF) which exhibits reduced SAR, good edge resolution and T<sub>2w</sub>, but is also insensitive to B<sub>0</sub> inhomogeneities.

**Methods:** Based on T<sub>2</sub>TIDE, T<sub>2</sub>VAPSIF incorporates a Kaiser-Bessel preparation module for transient signal stabilization and employs a PSIF acquisition scheme for reduced B<sub>0</sub> inhomogeneity sensitivity. The flip angle scheme thus consists of four blocks: i) Kaiser-Bessel (KB) stabilization pulses ii) 180° pulses iii) Ramp pulses and iv) PSIF (α) pulses. Partial Fourier fraction (PF) is used to adjust the effective TE (TE<sub>eff</sub>), thereby controlling the amount of T<sub>2w</sub>. The outer +k-space is acquired with PSIF as shown in Fig.1. MATLAB simulations were performed for T<sub>2</sub>TIDE and T<sub>2</sub>VAPSIF for 6 different tissues with T<sub>1</sub>/T<sub>2</sub> values (500/50, 500/60, 500/200, 2400/50, 2400/60, 2400/200 ms). Simulation parameters were #180: 25, #Ramp: 10, α: 70°, TR: 5.2 ms and off-resonance dephasing of -π to +π (steps of π/18). **Phantom Imaging:** All imaging was performed on a 3T MRI scanner (Siemens MAGNETOM Tim Trio). T<sub>2</sub> phantoms were prepared with different concentrations of MnCl<sub>2</sub>. 2D single slice TSE, HASTE, b-SSFP, T<sub>2</sub>-TIDE and T<sub>2</sub>VAPSIF images were acquired with similar spatial resolutions. T<sub>2w</sub> images were acquired with TE<sub>eff</sub> of 103ms and PF: 0.57. **Volunteer Imaging:** 2D single slice abdominal imaging was performed in two volunteers using respiratory triggered TSE (TE<sub>eff</sub>: 90ms) and HASTE, T<sub>2</sub>-TIDE and T<sub>2</sub>VAPSIF (TE<sub>eff</sub>: 180ms, PF: 0.69). An extra gradient of 50μT/m was applied along the read direction to induce B<sub>0</sub> inhomogeneities during T<sub>2</sub>-TIDE and T<sub>2</sub>VAPSIF acquisitions.

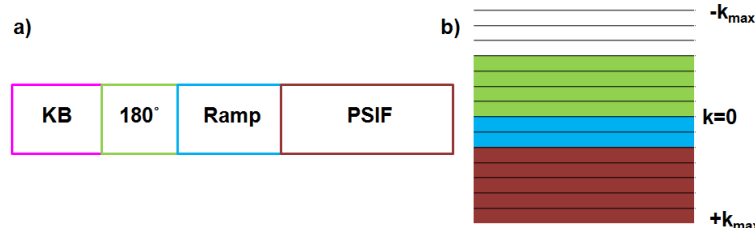
**Results:** Simulation results of T<sub>2</sub>-TIDE and T<sub>2</sub>VAPSIF (Fig.2) show that a) the initial 180° pulses result in pure T<sub>2</sub> decay which are ramped down to the SSFP/PSIF acquisition achieving a steady-state signal level and b) T<sub>2</sub>VAPSIF is insensitive to off-resonance related artifacts. Fig. 3 shows images of the phantom acquired using different sequences. Banding artifacts are visible in both b-SSFP (Fig.3c) and T<sub>2</sub>-TIDE (Fig.3d) (solid arrows) images, but not in T<sub>2</sub>VAPSIF (Fig.3f) images. T<sub>2</sub>VAPSIF also demonstrates comparable T<sub>2w</sub> to TSE and HASTE, with sharper edges than HASTE. Energy deposition of T<sub>2</sub>-TIDE and T<sub>2</sub>VAPSIF was reduced by a factor of 2 compared to HASTE. Volunteer images of T<sub>2</sub>TIDE (Fig.4c) show banding artifacts due to the extra gradient (white arrows), which are not seen with T<sub>2</sub>VAPSIF (Fig.4d). T<sub>2</sub>VAPSIF showed comparable T<sub>2w</sub> to TSE (Fig.4a) and HASTE (Fig.4b). Similar energy deposition was observed for both T<sub>2</sub>TIDE and T<sub>2</sub>VAPSIF



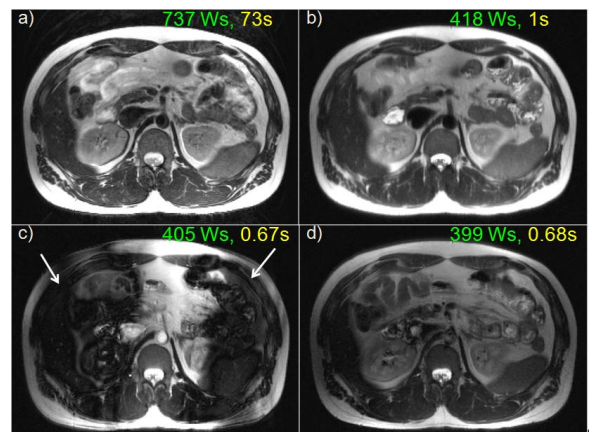
**Fig. 2:** Simulation of the normalized transverse magnetization at a given echo number for a) T<sub>2</sub>-TIDE b) T<sub>2</sub>VAPSIF with off-resonance of -π to π. The T<sub>1</sub>/T<sub>2</sub> values are shown in the legend.



**Fig. 3:** Phantom images acquired using a) TSE, b) HASTE, c) b-SSFP, d) T<sub>2</sub>-TIDE, e) T<sub>2</sub>TIDE PSIF with α/2 prep and f) T<sub>2</sub>VAPSIF. The banding artifacts (solid arrows) are strong in c)-e). Edge blurring (dashed arrows) is strong in b) and less so in f). The deposited energy (green) and acquisition duration (yellow) are shown above each image.



**Fig. 1:** a) Block diagram showing the flip angle scheme for the T<sub>2</sub>VAPSIF sequence b) k-space diagram showing the flip angle scheme with partial Fourier acquisition. Note: the Kaiser-Bessel (KB) block is used only for steady-state signal stabilization and no data is acquired. The 180 pulse block provides T<sub>2w</sub>; the Ramp and PSIF pulse blocks reduce SAR and maintain SNR in outer k-space lines.



**Fig. 4:** a) Respiratory-gated TSE b) HASTE c) T<sub>2</sub>-TIDE and d) T<sub>2</sub>VAPSIF. An additional 50 μT/m gradient was applied along the read direction during acquisition of c) and d) resulting in banding artifacts (white arrows) in c). The deposited energy and acquisition duration are shown above each image.

compared to HASTE but with a 1.5 factor reduction in acquisition duration.

**Conclusion:** T<sub>2</sub>VAPSIF is a promising sequence for fast, low SAR, T<sub>2w</sub> imaging that is insensitive to B<sub>0</sub> inhomogeneities and capable of good edge resolution.

**Reference:** 1. Paul D, et al., Proc. ISMRM 2005, 98.